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(54) Title: **EMBOLIZATION USING CARBON COATED PARTICLES**

(57) Abstract: Described are methods of embolization using an embolizing agent composition that includes particles with carbon surfaces, and comprising a contrast agent. Preferred particles include a radiopaque particle substrate and a pyrolytic carbon surface.

EMBOLIZATION USING CARBON COATED PARTICLES

Background

5 Therapeutic vascular occlusions (embolizations) are techniques used to treat certain pathological conditions in situ. Therapeutic embolization is practiced generally using a catheter, under imagery control, to position particulate embolization agents in the circulatory system, such as the vessels of various processes: tumors, vascular malformations, and hemorrhagic processes. Notably, vascular occlusion can suppress
10 pain or pressure sensations, limit blood loss (e.g., during a surgical intervention following embolization), or even prompt necrosis. In the case of vascular malformations, embolization can normalize blood flow to normal tissue, aid in surgery, and limit the risk of hemorrhage. In hemorrhagic processes, vascular occlusion produces a reduction of blood flow, which promotes cicatrization of arterial openings.
15 U.S. Pat. No. 5,635,215 discloses the use of hydrophilic acrylic copolymer microspheres coated with a cell adhesion promoter for therapeutic embolization.

 Uterine Artery Embolization (UAE) is the process of occluding the vascular blood supply to uterine fibroids to reduce fibroid size and alleviate associated symptoms, including bleeding, pain, and disfigurement. Fibroids are benign tumors of
20 smooth muscle. They are also called leiomyomas or myomas. Fibroids may arise in different parts of the uterus. They are named by their position within the uterus; submucosal, intramural, and subserosal. Some fibroids grow on a stalk and these are called pedunculated. Abnormal bleeding can be caused by submucosal or intramural fibroids. Intramural and subserosal fibroids can cause pelvic pain, back pain, and
25 generalized pressure sensations. Fibroids often fail to respond to medical therapies, causing either myomectomy (surgical removal of the fibroids) or hysterectomy to be an ultimate treatment.

 In recent years, there has been considerable research aimed at developing less invasive alternatives to surgical treatments of fibroids. One such alternative is uterine
30 fibroid embolization.

 PCT/GB98/02621 discloses a bio-compatible, embolizing agent comprising polymer particles such as polyvinyl alcohol, containing a contrast enhancing material.

The contrast enhancing materials can be located on the surface or in the pores of, or within micro-balloons formed from, the polymer particles. Consequently, the polymer particles retain a contrast enhancing effect in vivo for a prolonged period of at least seven days, or preferably at least fourteen days, and particularly preferably until the polymer particles biodegrade.

PCT/US99/04398 discloses a method for gynecological endovascular embolization with a fluid embolic composition that forms a coherent solid mass. The embolization agent is a composition of biocompatible polymers and a radiopaque material. In some applications where a water soluble radiopaque material is used, the composition does not contain any particles. The particle size is no more than 100 micrometers and preferably less than 10 micrometers.

U.S. Patent No. 4,999,188 (Solodovnik et al.) discloses a composition for embolization of blood vessels, in which agglomeration of particles is decreased as the composition is introduced. The proposed composition can additionally comprise a medicinal or radiopaque substance or a mixture of these in an amount of about 0.005 to about 8% by weight in relation to the total weight of the initial ingredients. The particles of the embolizing material may include particles of a polymer material moderately swelling in water, particles of glass or metal or a mixture thereof. Suitable polymeric particles include acetylcellulose, acetylphthalylcellulose, polyvinylacetate, copolymers of vinylpyrrolidone and methylmethacrylate.

U.S. Patent No. 5,202,352 (Okada et al.) discloses an intravascular embolizing agent containing an angiogenesis-inhibiting substance and an intravascular embolizing substance. The agent, with the administration of a relatively small dosage amount, enhances the anti-tumor effect of the angiogenesis-inhibiting substances. The addition of small doses of angiogenesis inhibiting substances also enhances the anti-tumor effect of intravascular embolizing agents.

U.S. Patent No. 5,236,410 (Granov et al.) discloses a method for tumor treatment which involves first catheterization of the vessel that supplies a tumor of interest. A suspension of a magnetically hard ferromagnetic substance in an oil solution of oil-soluble antitumor agent is then injected through the catheter under fluoroscopic control and, at the same time, local magnetic field is applied onto the tumor-bearing area. After 1-3 days, the tumor is subjected to oscillating power field

selected from ultrahigh radio frequency electromagnetic field and the field of ultrasonic contraction waves until the temperature of 43.0-43.5C is reached within the tumor, and this temperature is maintained for 5-45 minutes. In cases of large size tumors it is preferable to reduce the blood flow in the tumor-feeding blood vessel after the administration thereto of the suspension.

U.S. Patent No. 5,624,685 (Takahashi et al.) discloses a vascular lesion embolizing material comprising a high-polymer gel capable of absorbing water in an amount of 10 ml/g and more. When the high-polymer gel is supplied, either as such or after being bound with a binder or confined in a capsule, to the site of a blood vessel having a lesion to be repaired or its neighborhood, the gel swells upon contact with blood and spreads readily in the blood vessel to close the lumen of the blood vessels with lesion.

Summary of the Invention

In accordance with the present invention there is provided a method of embolization. The method includes the use of a composition that contains biocompatible particles comprising a carbon surface, preferably provided in a biocompatible carrier. The particles are preferably radiopaque, and are preferably in the range from about 100 microns to 1,000 microns in transverse, cross-sectional dimension. The composition may be designed to be delivered into the body through a small-bore needle, cannula, or catheter.

The carbon surface of the particles may be, for example, pyrolytic carbon, (such as isotropic carbon or low temperature isotropic carbon), vitreous carbon, or any other useful form of carbon. The carbon may be coated onto a particle substrate as a thin coating or film, thereby creating a particle that has a highly biocompatible, carbon surface. While not required, pyrolytic carbon may be preferred.

The material of the particle substrate may be but is not necessarily biocompatible, and should be capable of withstanding the conditions of the coating process, which might include elevated temperatures. In particularly preferred embodiments, particle substrates may be radiopaque most preferably permanently radiopaque. Exemplary materials for radiopaque particle substrates can include metals and metal oxides such as zirconium oxide and aluminum oxide. Carbon itself, such as

graphite or low temperature isotropic carbon, or other forms of carbon, may also be used as the particle substrate as well as other materials such as ceramics.

5 The fluid carrier may preferably be any biologically compatible material capable of delivering particles to a desired location, such as a biologically compatible suspension, solution, or other form of a fluid or gel. Specific examples of materials useful as biologically compatible carriers include saline, dextrans, glycerol, polyethylene glycol, and other polysaccharides or biocompatible polymers, either singly or in combination.

10 The use of the carbon-coated particles described herein has advantages over the use of other particles. Particles comprising a carbon coating, e.g., pyrolytic carbon, are very biocompatible. Preferred embodiments of the particle may be permanently radiopaque, e.g., by virtue of a radiopaque particle substrate. The location of the radiopaque particles can be monitored, by known methods, for as long as the radiopaque particles remain in a body. This is an improvement over many prior art contrast-enhancing agents which biodegrade or otherwise lose their radiopacity over a
15 period of days or weeks.

An aspect of the invention relates to a method for embolization, particularly gynecological embolization, including delivery of an embolic agent composition to a blood vessel to fill or plug the blood vessel and/or encourage clot formation so that
20 blood flow through the vessel is reduced or stopped. The embolic agent composition contains particles having a carbon surface. The carbon may preferably be pyrolytic carbon. The particles may preferably contain a contrasting agent, and are most preferably radiopaque by virtue of a permanently radiopaque particle substrate.

For purposes of the present disclosure, the following terms shall be given the
25 following meanings.

The term "biocompatible," refers to materials which, in the amount employed, are non-toxic and substantially non-immunogenic when used internally in a patient, and which are substantially insoluble in blood. Suitable biocompatible materials include ceramics, metals such as titanium, gold, silver, stainless steel, metal oxides,
30 carbon such as pyrolytic carbon or ultra low temperature isotropic carbon, etc.

The term "contrast-enhancing" refers to materials capable of being monitored during injection into a mammalian subject by methods for monitoring and detecting

such materials, for example by radiography or fluoroscopy. An example of a contrast-enhancing agent is a radiopaque material. Contrast-enhancing agents including radiopaque materials may be either water soluble or water insoluble. Examples of water soluble radiopaque materials include metrizamide, iopamidol, iothalamate sodium, iodomide sodium, and meglumine. Examples of water insoluble radiopaque materials include metals and metal oxides such as gold, titanium, silver, stainless steel, oxides thereof, aluminum oxide, or zirconium oxide.

Detailed Description

Embolization is a process wherein a material is injected into a blood vessel to at least partially fill or plug the blood vessel and/or encourage clot formation so that blood flow through the vessel is reduced or stopped (see background, supra). Embolization of a blood vessel can be useful for a variety of medical reasons, including preventing or controlling bleeding due to lesions (e.g., organ bleeding, gastrointestinal bleeding, vascular bleeding, and bleeding associated with an aneurysm), or to ablate diseased tissue (e.g., tumors, vascular malformations, hemorrhagic processes, etc.) by cutting off blood supply. Embolization may also be used to prevent blood loss during or immediately following surgery. Embolization of tumors may be performed preoperatively to shrink tumor size and to aid in visualization of a tumor and to prevent blood loss related to surgical procedures.

Emobilization may be used in treating skin, head, or neck tumors, tumors of the uterus or fallopian tubes, liver or kidney tumors, endometriosis, fibroids, etc. Particularly, embolization has been used for arteriovenous malformation of the pelvis, kidney, liver, spine and brain. Uterine artery embolization has been used for the treatment of fibroids; renal artery embolization has been used for the treatment of renal angiomyolipomas and renal cell carcinoma; intracranial embolization has been used for the treatment of cerebral and intracranial aneurysms, neuroendocrine metastases, intracranial dural arteriovenous fistula and patent ductus arteriosus. Other examples of specific procedures include hepatic artery embolization and pulmonary artery embolization. Examples of such procedures are described, e.g., in Mourikis D., Chatziioannou A., Antoniou A., Kehagias D., Gikas D., Vlahous L., "Selective Arterial Embolization in the Management of Symptomatic Renal Angiomyolipomas

(AMLs),” *European Journal of Radiology* 32(3):153-9, 1999 Dec.; Kalman D. Varenhorst E., “The Role of Arterial Embolization in Renal Cell Carcinoma,” *Scandinavian Journal of Urology & Nephrology*, 33(3):162-70, 1999 Jun.; Lee W., Kim TS., Chung JW., Han JK., Kim SH., Park JH., “Renal Angiomyolipoma: Embolotherapy with a Mixture of Alcohol and Iodized Oil,” *Journal of Vascular & Interventional Radiology*, 9(2):255-61, 1998 March-April; Layelle I., Flandroy P., Trotteur G., Dondelinger RF., “Arterial Embolization of Bone Metastases: is it Worthwhile?” *Journal Belge de Radiologie*, 81(5):223-5, 1998 Oct; Berman, MF., Hartmann A., Mast H., Sciacca RR., Mohr JP., Pile-Spellman J., Young WL., “Determinants of Resource Utilization in the Treatment of Brain Arteriovenous Malformations,” *Ajnr: American Journal of Neuroradiology*, 20(10):2004-8, 1999 Nov-Dec.; Shi HB., Suh DC., Lee HK., Lim SM., Kim DH., Choi CG., Lee CS., Rhim SC., “Preoperative Transarterial Embolization of Spinal Tumor: Embolization Techniques and Results,” *Ajnr: American Journal of Neuroradiology*, 20(10):2009-15, 1999 Nov-Dec.; Nagino M., Kamiya J., Kanai M., Uesaka K., Sano T., Yamamoto H., Hayakawa N., Nimura Y., “Right Trisegment Portal Vein Embolization for Biliary Tract Carcinoma: Technique and Clinical Utility,” *Surgery*, 127(2):155-60, 2000 Feb.; Mitsuzaki K., Yamashita Y., Utsunomiva D., Sumi S., Ogata I., Takahashi M., Kawakami S., Ueda S., “Balloon-Occluded Retrograde Transvenous Embolization of a Pelvic Arteriovenous Malformation,” *Cardiovascular & Interventional Radiology* 22(6):518-20, 1999 Nov-Dec.

While portions of the present description include language relating specifically to gynecological embolization, all types of embolization processes are considered to be within the contemplation of the present invention. Specifically, one of skill in the medical or embolizing art will understand and appreciate how carbon-coated particles as described herein can be used in various embolization processes by guiding a delivery mechanism to a desired vascular body site, and delivering of an amount of the particles to the site, to cause restriction, occlusion, filling, or plugging of one or more desired vessels and reduction or stoppage of blood flow through the vessels. Factors that might be considered, controlled, or adjusted for, in applying the process to any particular embolization process might include the chosen composition of the particles (e.g., to account for imaging, tracking, and detection of a radiopaque particle

substrate), the amount of particles delivered to the body site, the method of delivery, equipment used and the method and route used to place the dispensing end of the equipment at the desired body site. All of these factors will be appreciated by one of ordinary skill, and can be readily dealt with to apply the described methods to a large variety of embolization processes.

Embolization typically is performed using angiographic techniques and with guidance and monitoring, e.g., fluoroscopic or X-ray guidance, to deliver an embolizing agent to vessels or arteries. A vasodilator (for example adenosine) may be administered to the patient beforehand, simultaneously, or subsequently, to facilitate the procedure.

Gynecological embolization refers to embolization used to control acute and chronic genital bleeding in an obstetric or gynecological disorder, including uterine fibroids. Uterine Arterial Embolization (UAE) is a method of treating fibroids involving occluding uterine arteries that supply blood to the fibroid. Cutting off the blood supply reduces the size of the fibroid and alleviates symptoms such as bleeding, pain, and disfigurement.

At least two general variations of UAE are known. A first method, known generally as intravascular embolization, introduces or inserts a catheter through an artery, e.g., the femoral artery, and guides the catheter to a uterine artery. The second type of method inserts a catheter transcervically and guides the catheter into or through the uterine wall to directly access blood vessels to be embolized. The second method is considered to be less invasive and, accordingly, better tolerated as compared to intravascular methods.

Embolization procedures can typically include the following steps. A patient is sedated so as to be very sleepy during the procedure. For intravascular gynecological embolization, the uterine arteries can be accessed from the femoral artery, which is at the crease at the top of the leg. A needle can be used to puncture and enter the artery to provide access for a catheter. Local anesthesia can be used for this portion of the procedure. The catheter is advanced over the branch of the aorta and into the uterine artery on the side opposite the puncture, to a point where the artery divides into multiple vessels supplying blood to the uterus and uterine fibroids. The catheter can be steered through the artery by known techniques, e.g., using X-ray imaging, to guide the

catheter's progress. The procedure can be performed on both sides of the uterus so the blood supply is blocked in both the right and left uterine arteries. Some physicians block both uterine arteries from a single puncture site, while others puncture the femoral artery at the top of both legs, in which case a second arterial catheter is placed from the opposite femoral artery to the other uterine artery. Before starting delivery of the embolizing agent composition, an arteriogram is performed to provide a road map of the blood supply to the uterus and fibroids.

In a transcervical method, a catheter capable of penetrating a vessel to be embolized, such as a needle tipped catheter, is inserted through the cervix into the uterus using a device such as a hysteroscope, allowing visualization of the uterine wall. Generally, the patient is prepared in the usual manner for a hysteroscopic procedure, and a warm saline solution is infused to inflate the uterus and help visualize the uterine wall using the hysteroscope. Then the catheter is inserted through the scope. The vessel to be embolized is located and the catheter is inserted into or through the uterine wall and into the located vessel, e.g., the position of a uterine fibroid is determined and the needle tip of the catheter is placed in a blood vessel feeding or within the fibroid mass. Repeated placement of the catheter may be needed to completely embolize the vasculature of a uterine fibroid. Such a method is described in International Publication Number WO 99/43366.

The catheter delivering the embolizing agent composition may be a small diameter medical catheter. The particular catheter employed is not critical, provided that catheter components are compatible with the embolizing agent composition (i.e., the catheter components will not readily degrade in the embolizing agent composition, and vice versa). In this regard, polyethylene catheter components can be generally useful. Other materials compatible with the embolizing agent composition may include fluoropolymers (e.g., TeflonTM), silicone, etc.

Once a catheter is in place, an embolizing agent composition containing particles is injected through the catheter slowly, typically with the assistance of X-ray or fluoroscopic guidance. The particles are of a size that will effectively wedge in the vessels leading to the fibroids, occluding the vessel and reducing or preventing the flow of blood to the fibroid. The particles should also be of sufficient size that they do not remain mobile in the body. If the particles are too small, they can be engulfed by

the body's white cells (phagocytes) and carried to distant organs or be carried away in the microvasculature and travel until they reach a site of greater constriction. For the method of the present invention, preferred particles can have a transverse cross-sectional dimension between 100 and 1,000 micrometers.

5 The embolizing agent composition can be introduced directly into critical blood vessels (e.g., in the transcervical procedure), or they may be introduced upstream of target vessels (especially in an intravascular procedure). If introduced upstream from a target vessel, e.g., in fibroid embolization, the particles flow to the fibroids first, because the fibroids are very vascular. Over several minutes, the arteries are slowly
10 blocked. The embolization is continued until there is nearly complete blockage of blood flow in the vessel.

 The amount of embolizing agent composition, and particles, introduced during an embolization procedure can be an amount sufficient to cause embolization, e.g., to reduce or stop blood flow through the target vessels. The amount of embolizing agent
15 composition delivered can vary depending on the total of the vasculature to be embolized, the concentration and size of the microparticles.

 After embolization, another arteriogram can be performed to confirm the completion of the procedure. Arterial flow will still be present to some extent to healthy body tissue proximal to the embolization, e.g., to normal portions of a uterus,
20 while flow to the diseased or targeted tissue is blocked. The procedure can take approximately 1 to 1 ½ hours. As a result of the restricted blood flow, the diseased or targeted tissue, e.g., fibroids or tumors, begins to shrink.

 According to the invention, the embolizing agent composition comprises an injectable combination of particles in a biocompatible carrier.

25 The particles have a surface that comprises carbon. The carbon-containing particle surface may be in the form of a carbon-containing coating or carbon-containing film, e.g., isotropic carbon, pyrolytic carbon, or vitreous carbon, preferably in a form that is biocompatible. Various forms of carbon are described in the article "Material Properties and Applications of Pyrolite® Carbon," by Al Beavan, as
30 published in *Materials Engineering*, February 1990. Examples of carbon coated particles are described in United States Patent Number 5,792,478.

The atomic structure of both pyrolytic, e.g., LTI carbon, and vitreous carbon is similar to graphite, but the alignment between hexagonal planes of atoms is not as well ordered. Pyrolytic carbon is characterized by a more chaotic atomic structure with warped hexagonal planes, missing atoms, and generally a more turbostatic appearance.

5 This results in better bonding between layer planes.

The particles can preferably be constructed as a particle substrate having a carbon surface, e.g., a particle substrate having a layer of carbon coated thereon. While the substrate, need not be biocompatible due to its being coated with a preferably biocompatible layer comprising carbon, it may be preferred that the particle
10 substrate also be biocompatible.

The embolizing agent composition preferably comprises a contrast-enhancing agent which can be tracked and monitored by known methods, including radiography or fluoroscopy. The contrast-enhancing agent can be any material capable of enhancing contrast in a desired imaging modality (e.g. magnetic resonance, X-ray (e.g.
15 CT), ultrasound, magnetotomography, electrical impedance imaging, light imaging (e.g. confocal microscopy and fluorescence imaging) and nuclear imaging (e.g. scintigraphy, SPECT and PET)), and is preferably capable of being substantially immobilized within the particles, e.g., included in the particles as part of a carbon coating or as part of a particle substrate. Contrast-enhancing agents are well known in
20 the arts of embolization and similar medical practices, with any of a variety of such contrast-enhancing agents being suitable for use according to the methods of the invention.

Preferred embodiments of the invention can include a contrast-enhancing agent that is radiopaque in nature, in particular, a radiopaque material which exhibits
25 permanent radiopacity, as many metals or metal oxides do. Permanent radiopacity is unlike some other contrast-enhancing agents or radiopaque materials used in embolization or similar medical applications which biodegrade or otherwise lose their effectiveness (radiopacity) over a certain period, e.g., days or weeks, such as 7 to 14 days. (See, e.g., PCT/GB98/02621). Permanent radiopaque materials can be
30 monitored or tracked for as long as they remain in the body, whereas other non-permanent contrast-enhancing agents or radiopaque materials have a limited time during which they may be detected and tracked.

The contrast-enhancing agent may be incorporated into the microparticle as part of the particle substrate, as part of the carbon surface, or elsewhere. In one sense, a contrast-enhancing agent can be added to a material that is not detectable, e.g., not radiopaque, to make that material detectable. The contrast-enhancing agent may be provided in any such portion of a microparticle by known methods. According to a preferred mode of the invention, a permanent radiopaque material such as a metal or metal oxide may act as the particle substrate upon which a non-radiopaque carbon coating is placed. The particle substrates themselves are permanently radiopaque, and may permanently detected and tracked following deposition into the body.

Some examples of radiopaque materials include paramagnetic materials (e.g. persistent free radicals or more preferably compounds, salts, and complexes of paramagnetic metal species, for example transition metal or lanthanide ions); heavy atom compounds (i.e. atomic number of 37 or more), salts, or complexes (e.g. iodinated compounds, etc.); radionuclide-containing compounds, salts, or complexes (e.g. salts, compounds or complexes of radioactive metal isotopes or radiodinated organic compounds); and superparamagnetic particles (e.g. metal oxide or mixed oxide particles, particularly iron oxides). Preferred paramagnetic metals include Gd (III), Dy (III), Fe (II), Fe (III), Mn (III) and Ho (III), and paramagnetic Ni, Co and Eu species. Preferred heavy metals include Pb, Ba, Ag, Au, W, Cu, Bi and lanthanides such as Gd.

The amount of contrast-enhancing agent included in the particles should be sufficient to allow detection of the particles as desired. Preferably, particles of the embolizing agent composition comprise from about 10 to about 50 weight percent of contrast-enhancing agent, more preferably from about 20 to 40 weight percent contrast-enhancing agent, and even more preferably about 30 weight percent contrast-enhancing agent. Optionally, some, but not all particles used in a particular embolization procedure include a contrast-enhancing agent. Particles that include a permanent radiopaque particle substrate preferably have greater than 50 percent of their mass made up of the particle substrate.

The particles may be prepared using any of a variety of coating processes to deposit carbon onto a particle substrate. The particle substrate can be selected for compatibility with the coating process, meaning that it should be capable of withstanding temperatures used in a given process for coating carbon onto a particle

substrate. Relatively hard metallic or ceramic materials capable of withstanding high temperature conditions of a coating process can generally be preferred materials for the particle substrate. Metals, metal oxides, and alloys, including but not limited to medical grade stainless steel, titanium and titanium alloys, and oxide derivatives of stainless steel or titanium or titanium alloys, are also quite acceptable materials for the particle substrate, with aluminum oxide, and zirconium oxide being especially suitable. Carbon itself in any of its various forms, e.g., pyrolytic carbon, non-pyrolytic carbon, isotropic carbon, graphite, or vitreous carbon, may be useful as a particle substrate material. Thus, the particles may include a carbon coating deposited on a carbon particle substrate, and may be substantially or entirely made of carbon. In one embodiment of the invention, both the particle substrate and the carbon coating may comprise pyrolytic carbon.

The particle substrates, whatever their composition, should be of sufficient diameter, shape, and uniformity that they may be coated with carbon to produce carbon-coated particles of a size, quality, and nature as described herein. Optionally, the particle substrates, prior to coating, may be selected and processed, e.g., milled, extruded, sifted, cleaned, filtered, or otherwise formed, to provide a desired combination of particle size, shape, and quality to result in coated particles of a desired size, shape, and quality.

The carbon surface of the particles may comprise any form of carbon, with pyrolytic carbon, especially low temperature isotropic (LTI) pyrolytic carbon, being one preferred form. Pyrolytic carbon may be produced and coated onto a substrate surface by known methods. Generally, hydrocarbons and alloying gases are decomposed to prepare a pyrolytic carbon coating on a particle substrate. The particle substrates are included with the hydrocarbons and alloying gases in a fluidized or floating bed at a temperature sufficient to cause deposition of pyrolyzed carbon onto the substrate surface, e.g., from about 1200 to 1500°F. Inert gas flow is used to float the bed of particle substrates, optionally including an inert mixing media. The hydrocarbon pyrolysis results in a high carbon, low hydrogen content carbon material being deposited as a solid material on particle substrates.

Alternatively, a carbon coating (sometimes referred to as "ultra-low-temperature isotropic carbon") may be applied to a particle substrate using other

coating processes such as a vacuum vapor deposition process. This coating process effectively produces and deposits carbon onto a particle substrate using ion beams generated from any of a variety of known processes, such as the disassociation of CO₂, reactive dissociation in vacuum of a hydrocarbon as a result of a glow discharge, sublimation of a solid graphite source, or cathode sputtering of a graphite source. Gold has been found to be an especially suitable particle substrate for vacuum vapor deposited carbon. Other particle substrates including, but are not limited to, nickel, silver, stainless steel, or titanium.

The coating process is applied to substrate particles to produce final, preferably generally rounded, particles that have a smooth carbon-coated surface in the form of a thin coating or film. The resulting smooth surface enhances passage of the particles through an injection needle, cannula, or catheter. The high strength, resistance to breakdown or corrosion, and durability of the carbon surface ensures effective, long term functioning of the particles. The established biocompatibility of carbons such as pyrolytic and vitreous carbon makes the described particles particularly suitable for the embolization applications. In a preferred embodiment of carbon-coated particles, the particle substrates have been completely encased by a carbon surface. This results in a smooth coated particle with no substrate exposure on the surface of the particle or in contact with tissue when injected. Preferred carbon coatings can be in the range of fractions of thousandths of an inch, about one half of a thousands of an inch (0.0005 inches) on average, covering the surface of the particle substrate.

After the carbon coating has been deposited onto the particle substrate, the particles are subjected to a cleaning and sieving process to remove contaminants and to separate out particles of a size less than or greater than a desired size range. The particles may preferably range in size from 100 microns to 1,000 microns in average, transverse cross-sectional dimension, and a particularly preferred size range may be between 400 and 700 microns. The particles may be processed, e.g., segregated to a selected size range, for example using a sieving process such that the minimum particle dimension will pass through a U.S. No. 18 Screen Mesh (1000 micron grid size opening) but will not pass through a U.S. No. 140 Screen Mesh (106 micron grid size). That minimum dimension will be the transverse, cross-sectional dimension on

oblong or elongated particles, with that dimension coinciding with the particle diameter on generally spherical particles.

As stated, the carrier can be any biocompatible fluid capable of delivering the microparticles to a desired site. Examples of suitable materials for a carrier can

5 include saline, dextran, glycerol, polyethylene glycol, corn oil or safflower, or other polysaccharides or biocompatible organic polymers either singly or in combination. In use, the embolic agent composition may typically be injected in a fluid state, e.g., as a slurry, fluid suspension or emulsion, or as a gel, through a catheter, syringe needle, or cannula into a body site. When deposited into the blood stream, the carrier will
10 disperse or be absorbed in the body.

What is claimed:

1. A method for embolization comprising delivering an embolic agent composition to a blood vessel to fill or plug the blood vessel and/or encourage clot formation so that blood flow through the vessel is reduced or ceases, the embolic agent composition comprising particles comprising a carbon surface.
2. The method of claim 1 wherein the carbon surface comprises pyrolytic carbon.
3. The method of claim 1 wherein the carbon surface comprises low temperature isotropic pyrolytic carbon.
4. The method of claim 1 wherein the average, transverse cross-sectional dimension of the particles is between 100 and 1,000 micrometers.
5. The method of claim 1 wherein the particles comprise carbon-coated substrate particles and the substrate particles comprise a metal, a metal oxide, a ceramic, carbon, or a combination thereof.
6. The method of claim 1 wherein the particles comprise radiopaque substrate particles.
7. The method of claim 5 wherein the substrate particles comprise aluminum oxide, zirconium oxide, or a mixture thereof.
8. The method of claim 1 wherein the embolic agent composition further comprises a biocompatible carrier.
9. The method of claim 1 wherein the method comprises injecting the embolic agent composition into a uterine artery.

10. The method of claim 9 comprising introducing a catheter through a femoral artery.

11. The method of claim 9 comprising introducing the catheter transcervically, and
5 inserting the catheter through the uterine wall and into a blood vessel which feeds or is within a fibroid mass.

12. The method of claim 1 comprising the step of detecting the particle after
10 delivery to confirm placement at a designated site.

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